

OSTEOSYNTHESIS OF THE FRACTURED FIFTH METATARSUS WITH HEADLESS SCREW

K. Šimečková*, K. Frydryšek**, V. Machalla***, J. Demel****, L. Pleva*****, V. Bajtek*****

Abstract: *This article focuses on a fixative implant, namely a headless (Herbert) screw, designed for minimally invasive osteosynthesis of the 5th metatarsus. An original experiment is conducted in which the axial compression forces applied to the headless screw are measured and evaluated during osteosynthesis of the bone fragment in the laboratory. The information gathered fills in gaps in the knowledge of the measured quantities. The results of the experiment that have been made on porcine bones are compared with calculations using an analytical solution of a statically indeterminate task in compression.*

Keywords: headless (Herbert) screw, 5th metatarsus, osteosynthesis, experiments, analytical approach.

1. Introduction



Fig. 1: Radiograph of the fracture of the base of the 5th metatarsus after osteosynthesis by Herbert screw.

Osteosynthesis is an operative method for the treatment of complicated fractures consisting in fixation of bone fragments by means of implants (screws, splints, nails, wires, external fixators, etc.). These implants are introduced into the body temporarily or permanently. In our case, the fixation of the fracture by a headless screw is achieved by its design, due to the different pitch of the threads in the terminal threaded parts. This results in the mutual compression (tightening) of the fragments of the bone and subsequent healing.

The most common leg fractures are metatarsal fractures, and the most common type of these fractures are those of the 5th metatarsus, see Fig. 1, wherein the fixation of the fracture of the 5th metatarsus is performed by a Herbert type headless screw. These are the fractures of the base of the 5th metatarsus,

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which are most common amongst professional athletes (basketball, volleyball). The surgical treatment of these fractures improves their treatment and allows young athletes to return to the training process as soon as possible (Demel, 2004).

2. Progress of the experiment

The aim of the experiment was to determine the progress of the axial force acting on the headless self-cutting cannulated titanium alloy screw Ti;4,0/1,4x30/7 mm manufacture by MEDIN, a.s. This screw, shown in Fig. 2 (a), is made of titanium alloy Ti6Al4V, the properties of which are specified by the standard ISO 5832-3 (material for surgical implants). Knowledge of axial forces is an important element in the design and optimization of headless screws and their threads. In addition, there is insufficient information on such types of measurements in the literature (Šimečková, 2018).

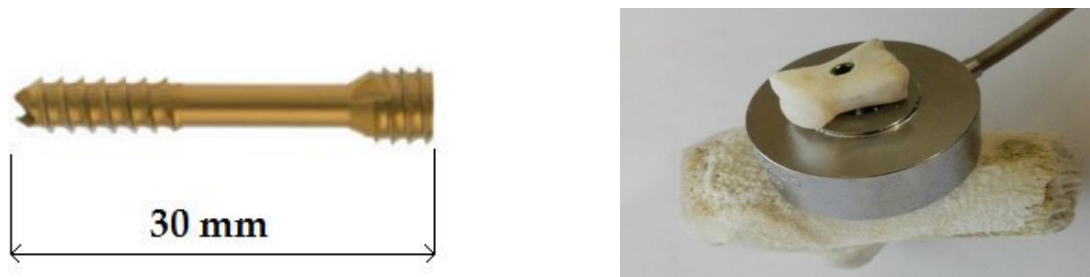


Fig. 2: (a) Dimensions of Headless Bone Screw; (b) Measurement (bone fragments, screw and sensor)

Using a strain gauge pressure sensor with an opening of LC 8150-375-500 type (see Fig. 2 (b)), the Vishay P-3500 strain indicator and the KRAFTWERK torque screwdriver, the axial compression forces applied to the headless screw during tightening were measured. The progress of the experiment was carried out in accordance with the surgical procedure. The experiment was performed on the headless screw introduced into the porcine leg bones. The porcine bone was used as an easily accessible and similar substitute for human metatarsus. Ten measurements were performed as a part of this research. The screw is tightened at a tightening torque of 2.5 Nm. Measurement of the force was carried out after the quarter of a turn of the screw until the headless screw was tightened to 3.5 turns and included the moment in which the thread in the bone is stripped (bone thread stripping - unsuccessful osteosynthesis).

3. Experiment results

All 10 measurements were statistically processed. The dependencies of the arithmetic mean, median, minimum and maximum of the compressive force F [N] on the tightening turns of the Herbert screw n [1] were determined. These dependencies are shown in Fig. 3 and 4 (for measurements 1 - 5 and 6 - 10) and Tab. 1.

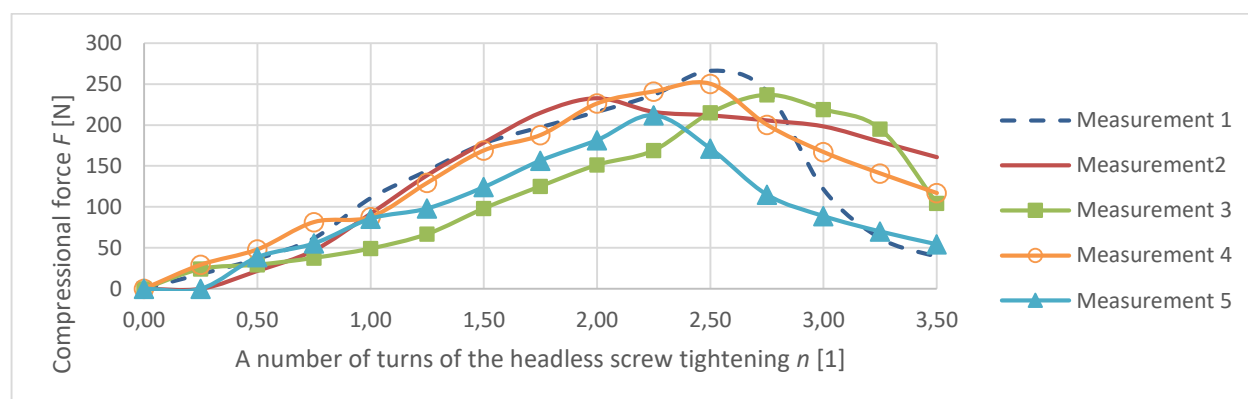


Fig. 3: Axial Force (measurement 1-5)

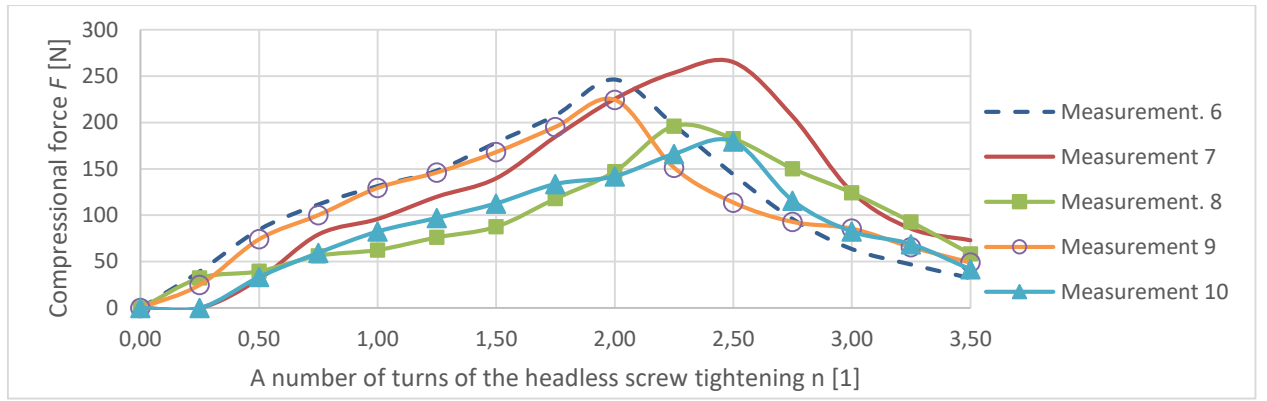


Fig. 4: Axial Force (measurement 6-10)

Tab. 1: Maximal measured values of axial forces.

Measurement	1	2	3	4	5	6	7	8	9	10	Mean (from Fig. 5)	Median (from Fig. 5)
<i>F</i> _{max} [N]	266	233	237	250	212	246	265	196	224	180	204	220
<i>n</i> [1]	2.5	2	2.75	2.5	2.25	2	2.5	2.25	2	2.5	2.25	2

Fig. 5 shows the course of the arithmetic mean and the median curve. The maximum and minimum force measurements constitute the envelope of the compression force dependency progress *F*. The highest average compressive force is 204 N and acts on the screw when tightened to 2.25 turns, then the thread is stripped in the bone and the compression force begins to decrease. The highest median value of the axial compressive force acts on the screw at 2 turns of tightening and its value is 220 N. It follows from the data that the safe limit for tightening the screw is 1.75 turns, which is the extreme value where no thread stripping has taken place at any measurements (i.e. important recommendations for physicians).

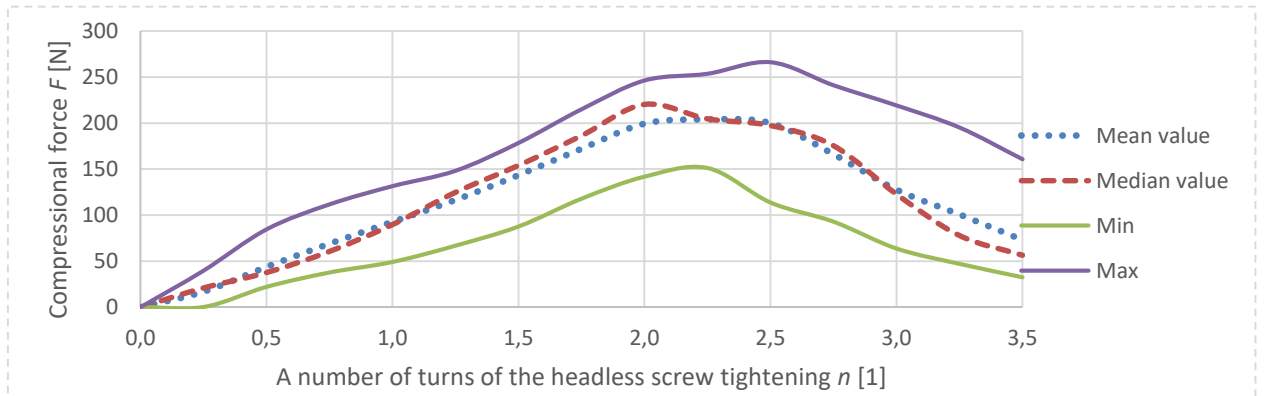


Fig. 5: Statistics of Axial Force

4. Comparison of measured values and analytical solutions

This task was also solved as 1× statically indeterminate compression task, assuming small deformations and using isotropic material (Šimečková, 2018). Normal force *F* for *n* = 1.75 of tightening turns was calculated as:

$$F = \frac{\Delta}{\frac{L_{k1}}{E_k \cdot A_{k1}} + \frac{1}{E_k} \left(\frac{L_b}{A_{k3}} + \frac{L_{k2} - L_b}{A_{k2}} \right) + \frac{1}{E_1} \left(\frac{L_a}{A_a} + \frac{L_b}{A_b} + \frac{L_c}{A_c} \right) + a_s} = 164.3 \text{ N.} \quad (1)$$

The meaning of each variable is given in Tab. 2. Comparison of the analytically calculated and measured normal force is also shown in Fig. 6. The figure shows that there is no significant variation in the analytical solution and measurement in the linear elastic region up to the tightening torque turns of the screw of 1.75, i.e. the thread is not stripped.

Tab. 2: Definition of quantities (Šimečková, 2018)

Quantity	Definition of quantity	Quantity	Definition of quantity
L_{k1}, L_{k2}	Lengths of bone fragments	Δ	Mutual displacement of the first bone fragment in respect of the second bone fragment after tightening
A_{k1}, A_{k2}, A_{k3}	Bone areas in individual parts of the screw	E_k	Modulus of tensile elasticity of the bone
A_a, A_b, A_c	Screw areas in individual parts	E_1	Modulus of tensile elasticity of the screw
L_a, L_b, L_c	Screw lengths in individual parts	a_s	Effect of the force sensor

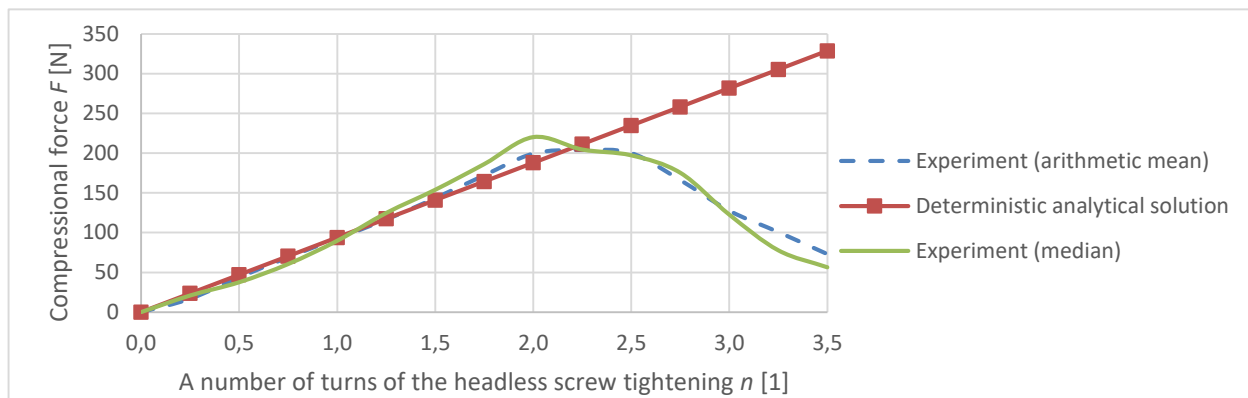


Fig. 6: Comparison of Measurement and Analytical Calculation

In Šimečková (2018) there is also an important stochastic solution of the problem using the Monte Carlo method, which is however not the subject of this article.

5. Conclusions

The main objective was to carry out an experimental analysis associated with the determination of axial force in osteosynthesis of 5th metatarsus with a headless screw (Ti;4.0/1.4x30/7 mm by MEDIN a.s.), which is intended to fix the 5th metatarsal fracture. Such fixation implants are commonly used in medical practice. It was found that the safe number of the tightening turns for this screw is 1.75. This value corresponds to the arithmetic mean of the measured axial force of 172 N or to the analytical calculated 164.3 N. The results obtained, similarly to the equivalent tasks solved in our facility, serve as testimonials for clinical tests, see e.g. Frydrýšek, 2018.

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References

- Šimečková, K. (2018) *Biomechanics: Implants in traumatology and orthopedics*. Diploma thesis, pp. 71, VŠB-TUO, Ostrava.
- Frydrýšek, K., Šír, M., Pleva, L. (2018) Strength Analyses of Screws for Femoral Neck Fractures, *Journal of medical and biological engineering*, Vol. 38, Issue:5, pp. 816-834, DOI:10.1007/s40846-018-0378-x
- Demel, J. Pleva L. (2004) Treatment of Jones fracture by Herebrt screw, *Úrazová chirurgie*, 2004, Vol II, ISSN 1211-7080.